Mathematical and Computational Modeling of Diffusion-Based Transport from Differing Designs of Drug Containing Sutures

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Outline

- Introduction
- Computational Methods
- Results
- Conclusions
- Suggestions?

GOAL: To investigate sutures as a drug delivery device to guide the stages of the wound healing process to promote healing and minimize scarring





Results of Literature Review



COMSOL Multiphysics, 5.0

$$\frac{\partial C_A}{\partial t} = D_A \left[\frac{\partial^2 C_A}{\partial x^2} + \frac{\partial^2 C_A}{\partial y^2} \right]$$

	Case 1	Case 2	Case 3
Study used in Interior Suture Domain	N/A	N/A	Time-dependent transport of diluted species
Study used in Porous Drug Coating or Porous Wall of Suture Domain	N/A	Time-dependent species transport in porous media (porosity = 0.3, 0.6, or 0.9)	Time-dependent species transport in porous media (porosity = 0.3, 0.6, or 0.9)
Study used in Wounded Dermal Tissue Domain	Time-dependent transport of diluted species	Time-dependent species transport in porous media (porosity = 1)	Time-dependent species transport in porous media (porosity = 1)



Case 1: Suture Design that Releases Drug through a Fixed Concentration Boundary



Case 2: Drug-Coated Solid Suture



Case 3: Drug-Loaded, Hollow Suture with Porous Wall



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Results of Each Case



Concluding Remarks

GOAL: To investigate sutures as a drug delivery device to guide the stages of the wound healing process to promote healing and minimize scarring

- COMSOL Modeling of Drug-Containing Sutures
 - Concentration profiles of drug simulant that might result from three designs of sutures
 - Results suggest time-varying effects associated with suture design
- Next Steps
 - Better match the suture designs to physiology by combining with experimental studies/physiological parameters



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Suggestions?

GOAL: To investigate sutures as a drug delivery device to guide the stages of the wound healing process to promote healing and minimize scarring

- COMSOL Modeling of Drug-Containing Sutures
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Extra Slides





- Species mass continuity equation
- Assumptions
 - Fick's Law of Diffusion
 - Diffusion in x- and ydirections only
 - No reaction occurring in the bulk of the domain



Dimensions of COMSOL Model		"Physics" for COMSOL Simulation		Parameters of COMSOL Simulation	
Width of Interior Suture Domain	N/A	Study used in Interior Suture Domain	N/A	Diffusion Coefficient of Drug Simulant	$1 * 10^{-10} \text{ m}^2/\text{s}$
Width of Porous Drug Coating or Porous Wall of Suture Domain	N/A	Study used in Porous Drug Coating or Porous Wall of Suture Domain	N/A	Permeability	N/A
Width of Wounded Dermal Tissue Domain	0.42 mm	Study used in Wounded Dermal Tissue Domain	Time- dependent transport of diluted species	Partition Coefficient	N/A
Height of Domain(s)	3 mm			Initial Concentration of Drug Simulant	1,000 mol/m ³ (Left Boundary)
				Initial Concentration of Drug Simulant Elsewhere	0 mol/m ³ 17

Dimensions and Para	ameters of Conceptual Domain	Parameters Used in COMSOL Simulation		
Assumed Width (Radius) of Interior Suture Domain	$6.0 * 10^{-4} \text{ m}$	Physics used in Wound Domain for COMSOL Simulation	Time-dependent transport of diluted species in porous media	
Calculated Width of Outer Transport Domain of Suture	3.25 * 10 ⁻⁵ m	Porosity Assumed for Wound Domain	0.1	
Width of Wounded Dermal Tissue Domain	4.2 * 10 ⁻⁴ m	Diffusion Coefficient of Drug Simulant	$1 * 10^{-11} \text{ m}^2/\text{s}$	
Height of All Domains	$3 * 10^{-3} \text{ m}$	Initial Concentration of Drug Simulant	900 mol/m ³ (Left Boundary)	
Assumed Initial Concentration of Drug Simulant in Interior Suture Domain	1,000 mol/m ³	Initial Concentration of	0 mol/m³ 18	
Assumed Initial Concentration of Drug Simulant in Outer Transport Domain of Suture	0 mol/m ³ (Allowed to quickly accumulate and not drop below 900 mol/m ³ during the duration of the validation simulation)	Elsewhere		

Dimensions of COMSOL Model		"Physics" for CO	MSOL Simulation	Parameters of COMSOL Simulation	
Width of Interior Suture Domain	N/A	Study used in Interior Suture Domain	N/A	Diffusion Coefficient of Drug Simulant	$1 * 10^{-10} \text{ m}^2/\text{s}$
Width of Porous Drug Coating or Porous Wall of Suture Domain	0.08 mm	Study used in Porous Drug Coating or Porous Wall of Suture Domain	Time-dependent species transport in porous media (porosity = 0.3, 0.6, or 0.9)	Permeability	1*10 ⁻⁶ m²/s
Width of Wounded Dermal Tissue Domain	0.42 mm	Study used in Wounded Dermal Tissue Domain	Time-dependent species transport in porous media (porosity = 1)	Partition Coefficient	1
Height of Domain(s)	3 mm			Initial Concentration of Drug Simulant	1,000 mol/m ³ (Drug-Coated Portion of Suture Domain)
				Initial Concentration of Drug Simulant Elsewhere	0 mol/m ³ 19

Dimensions of COMSOL Model		"Physics" for COMSOL Simulation		Parameters of COMSOL Simulation	
Width of Interior Suture Domain	0.2 mm	Study used in Interior Suture Domain	Time-dependent transport of diluted species	Diffusion Coefficient of Drug Simulant	$1 * 10^{-10} \text{ m}^2/\text{s}$
Width of Porous Drug Coating or Porous Wall of Suture Domain	0.08 mm	Study used in Porous Drug Coating or Porous Wall of Suture Domain	Time-dependent species transport in porous media (porosity = 0.3, 0.6, or 0.9)	Permeability	1*10 ⁻⁶ m²/s
Width of Wounded Dermal Tissue Domain	0.42 mm	Study used in Wounded Dermal Tissue Domain	Time-dependent species transport in porous media (porosity = 1)	Partition Coefficient	1
Height of Domain(s)	3 mm			Initial Concentration of Drug Simulant	1,000 mol/m ³ (Interior Suture Domain)
				Initial Concentration of Drug Simulant Elsewhere	0 mol/m ³ 20

Results of Case 1





Results of Case 1, Continued



Case 2: Drug-Coated Solid Suture Design



Results of Case 2, Continued





Results of Case 2





Results of Case 2, Continued



Case 3: Drug-Loaded, Hollow Suture with Porous Wall



Results of Case 3





Results of Case 3, Continued



Results of Case 3, Continued



Results of Case 3, Continued





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